Shear Bond Strength of Self-Adhesive Flowable Composite, Conventional Flowable Composite and Resin-Modified Glass Ionomer Cement to Primary Dentin

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ABSTRACT

Article type: Original Article

Objectives: This study aimed to compare the shear bond strength (SBS) of self-adhesive and conventional flowable composites and resin-modified glass-ionomer cement (RMGIC) to primary dentin.

Materials and Methods: In this in vitro, experimental study, the buccal surface of 48 primary canine and first molar teeth was longitudinally sectioned to expose dentin. The teeth were randomly divided into three groups (n=16) of 37.5% phosphoric acid+ OptiBond+ Premiere Flow composite (group 1), Vertise Flow composite (group 2) and RMGIC (group 3). A plastic cylindrical mold was placed on the exposed dentin and filled with restorative materials. The samples were then immersed in distilled water at 37°C for 24 hours, subjected to 1000 thermal cycles between 5-55°C and underwent SBS test. The mode of failure was determined under a stereomicroscope. Data were analyzed using one-way ANOVA and Tukey’s test.

Results: A significant difference was noted in SBS of the groups (P<0.05). The SBS of conventional flowable composite was significantly higher that of RMGIC and self-adhesive flowable composite (P<0.05). The difference in SBS of RMGIC and self-adhesive flowable composite was not significant (P>0.05). Failure at the dentin-restoration interface (adhesive failure) had the highest frequency in groups 1 and 2. The frequency of adhesive failure was 100% in group 3.

Conclusion: Within the limitations of this study, the conventional flowable composite yielded the highest SBS to primary dentin. Self-adhesive flowable composite and RMGIC showed the lowest SBS with no significant difference with each other.

Keywords: Composite Resins; Dentin; Glass Ionomer Cements; Shear Strength

INTRODUCTION

Tooth-colored restorative materials are increasingly used for tooth restoration due to excellent esthetics. Demand for tooth-colored restorations has greatly increased in pediatric dentistry. Conventional flowable composites and resin modified glass ionomer cements (RMGICs) are among the commonly used tooth-colored restorative materials with different mechanisms of adhesion to dental substrate [1]. Composite restorations have high technical sensitivity and high failure rate in primary teeth mainly due to the lack of cooperation of young children, which leads to inadequate isolation and subsequently decreased bond strength and increased microleakage [1]. Considering the
hydrophobicity of composite resins, their bonding to tooth structure has always been a challenge. Attempts have been made to change the morphology and chemical composition of tooth structure aiming to improve bond strength [2]. Conventional composite resins are bonded to dentin using the bonding systems, which aim to minimize marginal gap and increase the fracture strength and durability of restorations [3]. Researchers are trying to simplify the bonding procedure, and all-in-one bonding agents have been introduced that contain etchant, primer and adhesive all in one bottle to simplify the procedure of composite restoration [4]. Recently, self-adhesive flowable composites were introduced to the market that possess the advantages of all-in-one bonding systems and flowable composites altogether [4-6]. The clinical advantages of this type of composite include easy use (not requiring separate etching, priming or adhesive application), prevention of procedural errors related to clinical application of conventional bonding agents (such as over-drying and over-wetting) and reduction of chair time [4-7]. However, durability and clinical service of these composites remain a concern for many dental clinicians [8]. Studies on physical and mechanical properties of self-adhesive composites are limited [5, 6, 9, 10] and studies on the bonding properties and other characteristics of self-adhesive flowable composites in primary teeth are scarce [11]. Considering all the above, this study aimed to assess the shear bond strength (SBS) of self-adhesive flowable composite, conventional flowable composite and RMGIC to primary dentin. The mode of failure was also determined under a stereomicroscope.

**MATERIALS AND METHODS**

This in vitro, experimental study evaluated 48 extracted primary canine and first molar teeth. The study was approved in the ethics committee of our university (code: IR.TUMS.DENTISTRY.REC.1396.3345). Sample size was calculated to be 12 in each of the three groups according to a study by Sachdeva et al, [11] using one-way ANOVA power analysis feature of PASS 11 software assuming alpha=0.05, beta=0.2, standard deviation of 2.11 and effect size of 0.56. To increase the accuracy of the results, 48 teeth (n=16 in each group) were evaluated in this study. All teeth were collected within 3 months and stored in distilled water. The inclusion criteria were primary canine and first molars close to their physiologic exfoliation time, over-retained teeth and teeth that were candidates for serial extraction. Teeth with developmental anomalies, extensive caries, and with broken crowns were excluded. The teeth were immersed in 0.5% chloramine T solution for 7 days. After disinfection, the teeth were rinsed with distilled water, dried and mounted in polyester blocks so that their longitudinal axis was perpendicular to the surface. After mounting, a longitudinal section was made at the buccal surface to expose dentin using a cutting machine (T201A Mecatome; Presi, France). The teeth were then cleaned, rinsed and dried. The samples were randomly divided into three groups of 16 for the use of three restorative materials. Table 1 shows the characteristics of the three restorative materials used in this study.

RMGIC (Ionolux, Voco, Germany) was used in group 1. No surface treatment was performed on dentin. The glass ionomer powder and liquid were mixed in 3.2/1 g ratio or one scoop of powder and two drops of liquid according to the manufacturer’s instructions. Mixing time was 30 seconds. After mixing, the homogenous paste was packed into a cylindrical transparent plastic mold with an internal diameter of 3 mm and 2 mm height to reach 2 mm thickness. Care was taken to avoid void formation. Light curing was then performed using a LED light curing unit (Blue Phase; Ivoclar Vivadent, Schaan, Lichtenstein) with a light intensity of 600 mW/cm² for 20 seconds. After polymerization, plastic molds were removed using a scalpel. Conventional flowable composite (Premise Flow; Kerr, Bolzano, Italy) was used in group 2. Dentin was etched with 37.5% phosphoric acid (Kerr, Bolzano, Italy) for 15 seconds. The etched area was rinsed with distilled water, dried, and a drop of OptiBond (Kerr, Bolzano, Italy) was applied on the dentin surface with a microbrush.
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according to the manufacturer's instructions. It was rubbed on the surface and gently air-sprayed for 3 seconds. Light curing was performed for 20 seconds.

Flowable composite was applied into the transparent cylindrical plastic molds with 2 mm thickness and polymerized for 20 seconds. The mold was then removed using a scalpel.

Table 1. Characteristics of the three restorative materials used in this study

<table>
<thead>
<tr>
<th>Material</th>
<th>Composition</th>
</tr>
</thead>
</table>
| Premise Flow (Kerr) conventional flowable composite | Prepolymerized filler (PPE)  
Barium glass  
Silica filler  
Ethoxylated bis-DMA  
TEGDMA  
Light cure initiators and stabilizer  
Organophosphate dispersant |
| Acid etchant (Kerr)                                | 37.5% phosphoric acid  
Silica thickener |
| OptiBond bonding agent (Kerr)                      | Bis-GMA, HEMA, GPDM, photo-initiators  
Fillers  
Ethanol |
| Vertise Flow self-adhesive flowable composite (Kerr) | GPDM*, HEMA*, MEHQ*, zinc oxide  
Filler content |
| Ionolux resin modified glass ionomer cement (Voco) | Powder: polyacrylic acid, fluorosilicate glass, amine  
liquid: HEMA, polyacrylic acid, glycerin dimethacrylate, UDMA, BHT |

GPDM: Glycerol phosphate dimethacrylate; HEMA: Hydroxyethyl methacrylate; MEHQ: 4- methoxyphenol

Self-adhesive flowable composite (Vertise, Kerr, Italy) was used in group 3. In this group, first a 0.5 mm increment was applied on the dentin surface and rubbed with moderate pressure using a microbrush for 15 to 20 seconds. This layer was cured for 20 seconds. The next increment was applied in 1.5 mm thickness and curing was performed for 20 seconds. The mold was then removed. Care was taken to prevent void or crack formation in samples. The teeth were immersed in distilled water at 37°C for 24 hours and thermocycled for 1000 cycles between 5-55°C in a thermocycler (TC-300; Vafaei Industrial, Tehran, Iran) with a dwell time of 30 seconds and transfer time of 5 seconds [12]. The SBS was measured using a universal testing machine (Z250; Zwick/Roell, Germany). Load was applied with a blade perpendicular to the tooth-restoration interface at a crosshead speed of 1 mm/minute and the load cell applied load until bond failure. The mode of failure was evaluated under a stereomicroscope (SMZ800; Nikon, Tokyo, Japan) at x20 magnification. The mode of failure was categorized as adhesive (at the dentin-restorative material interface), cohesive (within the restorative material or dentin substrate) or mixed (a combination of both adhesive and cohesive failures).

Data were analyzed using SPSS version 22 (SPSS Inc., IL, USA). One-way ANOVA was applied to compare the SBS among the three groups. Tukey's post hoc test was applied for pairwise comparisons. P<0.05 was considered statistically significant.

RESULTS

Table 2 shows the mean and standard deviation of SBS in the three groups. The highest SBS was noted in the conventional flowable composite (14.87±3.4 MPa) while the lowest SBS was noted in RMGIC group (5.39±2.6 MPa). One-way ANOVA showed a significant difference in SBS among the three groups (P<0.001).

Table 2. Mean and standard deviation (SD) of shear bond strength (MPa) in the three groups (n=16)

<table>
<thead>
<tr>
<th>Study group</th>
<th>Min</th>
<th>Max</th>
<th>Mean</th>
<th>SD</th>
</tr>
</thead>
<tbody>
<tr>
<td>Conventional flowable composite</td>
<td>7.12</td>
<td>18.99</td>
<td>14.87</td>
<td>3.42</td>
</tr>
<tr>
<td>Self-adhesive flowable composite</td>
<td>3.69</td>
<td>9.92</td>
<td>6.60</td>
<td>1.97</td>
</tr>
<tr>
<td>Resin-modified glass ionomer cement</td>
<td>0.53</td>
<td>9.35</td>
<td>5.39</td>
<td>2.63</td>
</tr>
</tbody>
</table>

* The mean difference is significant at the 0.05 level.  
RMGIC: Resin-modified glass ionomer cement; Flow: Conventional flowable composite; Vertise: Self-adhesive flowable composite
Table 3. Pairwise comparisons of the groups in terms of shear bond strength

<table>
<thead>
<tr>
<th>(I) groups</th>
<th>(J) groups</th>
<th>Mean Difference (I-J)</th>
<th>Significance</th>
<th>95% Confidence Interval</th>
<th>Lower Bound</th>
<th>Upper Bound</th>
</tr>
</thead>
<tbody>
<tr>
<td>Resin-modified glass ionomer cement (RMGIC)</td>
<td>Flow</td>
<td>-9.49*</td>
<td>&lt;0.001</td>
<td>-11.84</td>
<td>-7.14</td>
<td></td>
</tr>
<tr>
<td></td>
<td>Vertise</td>
<td>-1.22</td>
<td>.429</td>
<td>-3.57</td>
<td>1.14</td>
<td></td>
</tr>
<tr>
<td>Conventional flowable composite (Flow)</td>
<td>RMGIC</td>
<td>9.49*</td>
<td>&lt;0.001</td>
<td>7.14</td>
<td>11.84</td>
<td></td>
</tr>
<tr>
<td></td>
<td>Vertise</td>
<td>8.27*</td>
<td>&lt;0.001</td>
<td>5.92</td>
<td>10.62</td>
<td></td>
</tr>
<tr>
<td>Self-adhesive flowable composite (Vertise)</td>
<td>RMGIC</td>
<td>1.22</td>
<td>.429</td>
<td>-1.14</td>
<td>3.57</td>
<td></td>
</tr>
<tr>
<td></td>
<td>Flow</td>
<td>-8.27*</td>
<td>&lt;0.001</td>
<td>-10.62</td>
<td>-5.92</td>
<td></td>
</tr>
</tbody>
</table>

* The mean difference is significant at the 0.05 level

Table 3 shows pairwise comparisons of the groups in terms of SBS. Tukey’s HSD post-hoc test showed that conventional flowable composite had a significantly higher SBS to primary dentin compared to the other two groups (P<0.001). Self-adhesive flowable composite and RMGIC groups showed the lowest SBS, with no significant difference with each other (P=0.429). Table 4 shows the mode of failure of samples in the three groups.

Table 4. Mode of failure in the three groups (n=16)

<table>
<thead>
<tr>
<th>Group</th>
<th>Adhesive</th>
<th>Mixed</th>
<th>Cohesive</th>
</tr>
</thead>
<tbody>
<tr>
<td>Conventional flowable composite</td>
<td>11</td>
<td>5</td>
<td>0</td>
</tr>
<tr>
<td>Self-adhesive flowable composite</td>
<td>13</td>
<td>3</td>
<td>0</td>
</tr>
<tr>
<td>Resin-modified glass ionomer cement</td>
<td>16</td>
<td>-</td>
<td>0</td>
</tr>
</tbody>
</table>

The adhesive type was the most frequent mode of failure in the conventional composite and self-adhesive groups. Adhesive failure was noted in 100% of samples in RMGIC group (Fig. 1).

DISCUSSION

This study assessed and compared the SBS of self-adhesive flowable composite, conventional flowable composite and RMGIC to primary dentin. A significant difference was noted in SBS of the groups. Our findings showed that the SBS of conventional flowable composite was significantly higher than that of self-adhesive flowable composite, which is in agreement with the results of previous studies [4,7,9,11,13-15]. Our findings showed that the SBS of conventional flowable composite was significantly higher than that of self-adhesive flowable composite, which is in agreement with the results of previous studies [4,7,9,11,13-15]. Etch and rinse bonding system was used for the conventional composite in our study. Separate etching eliminates the smear layer and mineral contents of dentin to 5-8 µ depth [16]. It increases the permeability of dentin and enhances subsequent penetration of adhesive monomers [17]. Formation of the hybrid layer at the interface of intertubular demineralized dentin and bonding agent enhances the physical properties [18]. Also, etching with phosphoric acid in etch and rinse systems results in formation of longer and thicker resin tags compared to those in self-etch systems (as in self-adhesive flowable composites) [11]. Two types of functional monomers are involved in the bonding mechanism of self-adhesive composites namely hydroxyethyl methacrylate (HEMA) and glycerol phosphate dimethacrylate (GPDMA). HEMA is responsible for reaction with other methacrylate monomers and since it is hydrophilic, it enhances resin adhesion by enhancing the wetting of dentin. Thus, it can effectively increase the bond strength.
Studies regarding the reaction of GPDMA monomer with dentin hydroxyapatite are limited [19]. However, it seems that GPDMA monomer can etch the enamel and dentin [8]. However, the acidity of Vertise Flow is not high enough to modify the smear layer and allow the penetration of resin into the substrate. Resultantly, the micromechanical retention would be lower and subsequently a lower bond strength is achieved by self-adhesive composite resins [20].

The manufacturer of OptiBond claims that it contains 15% barium glass filler (0.04 µ) that not only reinforces the hybrid layer but also penetrates well into dentinal tubules and forms a structural bonding, which is not seen in unfilled or nanofilled composite resins. This filler increases the bond strength to tooth surfaces and prevents microleakage. This can also explain the higher bond strength of conventional composite/OptiBond compared to self-adhesive composite with no separate bonding agent. Premise Flow conventional composite has low-viscosity TEGDMA monomer in its composition. Since this monomer is a cross-linker, it can effectively increase the bond strength and enhance the penetration of resin into the dentin structure [21].

Uekusa et al. [22] stated that the smear layer is rapidly removed by etching of primary dentin. Thus, shorter etching time by using a weaker etchant is recommended for primary teeth. However, etch and rinse bonding systems have phosphoric acid as etchant, which is a strong acid and can be more invasive for primary dentin. Also, due to lower thickness of dentin in primary teeth, it can cause exposure of dense and wide dentinal tubules close to dental pulp and consequently limit the efficacy of bonding process. Therefore, self-adhesive composite systems are expected to be suitable for application on primary dentin due to their lower acidity than etch and rinse systems.

However, our results showed higher bond strength of conventional composite and etch and rinse bonding system to primary dentin, which may be due to high viscosity and absence of solvent in self-adhesive flowable composite and its subsequent limited penetration into dentin structure [7].

Thus, it may be concluded that high viscosity, less wettability and limited penetration of self-adhesive composites can result in lower bond strength compared to the use of conventional composites and total etch bonding systems [23]. Our findings also revealed lower SBS of RMGIC than that of conventional flowable composite, which was in line with the findings of a previous study [13]. Studies comparing the bond strength of RMGIC and self-adhesive composite are scarce. In our study, the SBS values of RMGIC and self-adhesive composite were comparable; this finding was in agreement with that of Pacifici et al. [13] and Scaminaci et al [14]. RMGIC and self-adhesive composite have easier application than the conventional composite. Application of self-adhesive composite is even easier and faster than RMGIC. Although self-adhesive composite does not release fluoride, it has high filler content and is believed to have a higher wear resistance than RMGIC. Moreover, Vertise Flow composite has a less porous surface than RMGIC, which can result in higher esthetics and less plaque accumulation.

Decreased postoperative tooth hypersensitivity is another advantage of Vertise self-adhesive composite [7,13]. Scaminaci et al. [15] reported that the SBS of Vertise Flow was significantly higher than that of glass ionomer cement, which was in contrast to our finding. This difference in the results may be due to the use of conventional cement (Ketac Fil), which has a lower SBS than RMGIC, which can result in higher esthetics and less plaque accumulation.

With regard to the mode of failure, stereo-microscopic assessment in our study showed that the adhesive type had the highest frequency, which can be due to several factors such as inadequate degree of conversion of monomer/polymer [24], inadequate wetting of

Makishi et al. [9] evaluated confocal laser scanning microscopy images and did not detect formation of hybrid layer following the use of Vertise Flow composite.
dentin with bonding agent, no formation of hybrid layer or formation of a thin, non-homogenous hybrid layer [25]. Considering the presence of chemical bonding mechanism between glass ionomer cement and dentin, the adhesive bond at the interface is expected to be stronger than the cohesive bond within the cement. However, considering the dominant mode of failure being the adhesive type in RMGIC group, it seems that high viscosity of this material causes less mechanical interlocking and consequently less contact of material with the porosities and irregularities of the dentin surface. This study had an in vitro design. Oral conditions cannot be well simulated in vitro in terms of thermal changes, masticatory forces, water sorption, and pH alterations. Thus, generalization of results to the clinical setting must be done with caution. Future in vivo studies are required to compare the clinical success of these restorative materials in a larger sample size.

CONCLUSION
Within the limitations of this study, the conventional flowable composite yielded the highest SBS to primary dentin. Self-adhesive flowable composite and RMGIC showed the lowest SBS with no significant difference with each other.

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